

1 Prophylaxis of *Mycobacterium tuberculosis* H37Rv Infection in a Preclinical Mouse
2 Model via Inhalation of Nebulized Bacteriophage D29

3

4 Nicholas B. Carrigy,^{a†} Sasha E. Larsen,^{b†} Valerie Reese,^b Tiffany Pecor,^b Melissa
5 Harrison,^c Philip J. Kuehl,^d Graham F. Hatfull,^e Dominic Sauvageau,^c Susan L. Baldwin,^b
6 Warren H. Finlay,^a Rhea N. Coler,^{b,f,g} Reinhard Vehring^{a#}

7

8 ^aDepartment of Mechanical Engineering, University of Alberta, Edmonton, Canada

9 ^bInfectious Disease Research Institute, Seattle, USA

10 ^cDepartment of Chemical and Materials Engineering, University of Alberta, Edmonton,
11 Canada

12 ^dLovelace Biomedical, Albuquerque, USA

13 ^eDepartment of Biological Sciences, University of Pittsburgh, Pittsburgh, USA

14 ^fDepartment of Global Health, University of Washington, Seattle, USA

15 ^gPAI Life Sciences Inc., Seattle, USA

16

17 Running Title: Phage D29 Inhalation Provides Protection against TB

18

19 [#]Address correspondence to Reinhard Vehring, reinhard.vehring@ualberta.ca

20 [†]NC and SL contributed equally to this work

21 **Abstract**

22 Globally, more people die annually from tuberculosis than from any other single
23 infectious agent. Unfortunately, there is no commercially-available vaccine that is
24 sufficiently effective at preventing acquisition of pulmonary tuberculosis in adults. In this
25 study, pre-exposure prophylactic pulmonary delivery of active aerosolized anti-
26 tuberculosis bacteriophage D29 was evaluated as an option for protection against
27 *Mycobacterium tuberculosis* infection. An average bacteriophage concentration of
28 approximately 1 PFU/alveolus was achieved in the lungs of mice using a nose-only
29 inhalation device optimized with a dose simulation technique and adapted for use with a
30 vibrating mesh nebulizer. Within 30 minutes of bacteriophage delivery, the mice
31 received either a low dose (~50-100 CFU), or an ultra-low dose (~5-10 CFU), of *M.*
32 *tuberculosis* H37Rv aerosol to the lungs. A prophylactic effect was observed with
33 bacteriophage aerosol pre-treatment significantly decreasing *M. tuberculosis* burden in
34 mouse lungs 24 hours and 3 weeks post-challenge ($p < 0.05$). These novel results
35 indicate that a sufficient dose of nebulized mycobacteriophage aerosol to the lungs may
36 be a valuable intervention to provide extra protection to health care professionals and
37 other individuals at risk of exposure to *M. tuberculosis*.

38 **Keywords:** experimental therapeutics, global health, *in vivo* murine model, nose-only
39 inhalation device, phage prophylaxis, vibrating mesh nebulizer

40 **Introduction**

41 The World Health Organization (WHO) has classified the bacterium *Mycobacterium*
42 *tuberculosis* (*Mtb*) as the leading infectious killer globally for a fourth consecutive year
43 (1). Aside from being a significant co-morbidity in persons living with human
44 immunodeficiency virus (HIV), in both 2016 and 2017 tuberculosis (TB) was the cause
45 of death for 1.3 million persons without HIV infection (1). Not only do low-income
46 countries continue to suffer from endemic TB, but so do some populations in developed
47 countries such as Indigenous peoples in Nunavut, Canada (2).

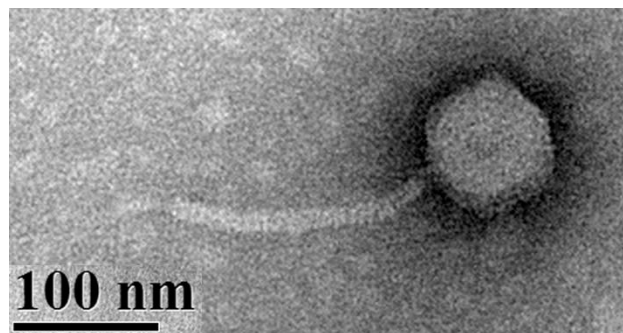
48 The global community is increasingly concerned about the increase of drug-resistant
49 *Mtb* strains. The WHO estimated that, in 2017, roughly 0.5 million *Mtb* infected
50 individuals developed rifampicin resistance and over 80% of those cases were
51 considered multidrug-resistant (1). As global treatment success for drug-resistant *Mtb*
52 cases remains unacceptably low - at roughly 55% -, alternative interventions that block
53 transmission and subsequent new infections are urgently needed (1). Vaccines against
54 *Mtb* are an active area of research (1,3-6), and indeed much of the global community
55 receives bacille Calmette–Guérin (BCG) vaccination against TB as youth. BCG and
56 other vaccine candidates can induce limited prophylactic protection through
57 adolescence (7); however, BCG provides limited-to-no prophylactic effect if given to
58 adults, does not prevent reactivation of latent TB, and does not prevent *Mtb*
59 transmission (8,9). Indeed, there is no vaccine that effectively prevents acquisition of
60 *Mtb* and progression to TB disease in adults (1). The lengthy, complex, multidrug
61 treatment regimens available to target active TB often result in poor side-effects for
62 patients. This limits adherence and perpetuates the development of drug resistance.

63 Epidemiologic vulnerability to TB disease correlates with proximity to an active case or
64 intensity of exposure over time. This is evidenced in highly-exposed health care workers
65 who have a 2-4 fold higher infection risk compared to medical students with low
66 exposure (10). Indeed, many studies document the increased risk to health care
67 workers (11,12), which justifies research toward the development of interventions
68 against *Mtb* infection for this high-risk population. Bacteriophage (phage) delivery may
69 be leveraged as an adjunct to current preventative strategies, which include personal
70 protective equipment, administrative and environmental controls (13,14), for health care
71 professionals who are regularly exposed to infectious active cases of TB.

72 Phages are diverse viruses that have co-evolved with bacteria and represent the most
73 common biologic on earth (15). Phage strains are host- and receptor-restricted and
74 therefore only capable of infecting a narrow-spectrum of bacteria, which notably results
75 in minimal harm to host microbiomes such as gut flora (16). Furthermore, antibiotic-
76 resistance does not influence bacterial susceptibility to phage lysis (16), making phages
77 an attractive tool against drug-resistant organisms. Phages predicted to use obligatory
78 lytic life cycles can be distinguished from temperate phages through genetic analysis
79 (17). The lytic cycle encompasses injection of phage DNA into the cell, phage
80 replication, and lysis of the bacterial cell wall to release the progeny. Lytic phage
81 therapy is considered safe and regularly utilized clinically in Eastern Europe, where
82 some phage cocktails are available without prescription (18). Indeed, studies have
83 repeatedly demonstrated that phages are not inherently harmful to humans (19).

84 Phage therapy is a viable option for compassionate use in the United States, with a
85 recent study demonstrating successful treatment of a patient with disseminated

86 multidrug-resistant *Acinetobacter baumannii* infection (20). In the United Kingdom, a
87 cystic fibrosis patient with disseminated *Mycobacterium abscessus* recently showed
88 objective clinical improvement with intravenous three-phage cocktail treatment (21). The
89 treatment of pulmonary infections in humans using phages has been reviewed
90 elsewhere (22). Advanced research of aerosol phage therapy has become prevalent,
91 including *in vitro* studies evaluating phage delivery with nebulizers, dry powder inhalers,
92 and pressurized metered-dose inhalers (23-31). As more than 80% of TB cases
93 originate from *Mtb* infections in the lungs, aerosol delivery of phage may be an ideal
94 mechanism for enabling activity at the primary site of *Mtb* infection (32). Note that phage
95 aerosol delivery without the use of additional vectors is unlikely to have efficacy against
96 *Mtb* already harboured within a granuloma; even phage infection of *Mtb* within a
97 macrophage, the primary target cell of *Mtb*, has low efficiency (33). However,
98 prophylactic delivery of phages to the alveoli may allow the phage to infect the
99 mycobacteria before macrophage uptake (17,27,34). Since the lungs contain millions of
100 alveoli, a high dose of active phage is likely required for prophylaxis. Of particular
101 interest for prophylactic protection against TB is *Siphoviradae* mycobacteriophage D29
102 (Figure 1), which can effectively infect and lyse a range of mycobacteria, including *Mtb*
103 (35).



104

105 **Figure 1.** Transmission electron micrograph of phage D29. The icosahedral capsid
106 contains double-stranded DNA. The tail is flexible and does not contract during
107 infection. The method for imaging is described elsewhere (27).

108 Before testing the efficacy of phage D29 aerosol in humans, animal studies are of
109 interest. Laboratory mice, commonly used for studying drug efficacy, have the
110 advantages of low cost, short growth time, and small size, allowing for many mice to be
111 tested simultaneously (36). Different methods for delivering aerosol to mice include a
112 nose-only inhalation device (NOID), whole-body exposure system, nose-drip, and
113 intranasal or intratracheal instillation. Use of a NOID is the most common exposure
114 method for rodents as it allows for a uniform distribution of aerosol in the lungs via the
115 nasal inhalation route, which is applicable to rodents as they are obligate nasal
116 breathers (37-39). Whole-body exposure systems require larger doses as they are
117 inefficient and cause aerosol deposition on the body of the mouse (36,38,40). Nose-drip
118 methods do not simulate natural aerosol inhalation and have variable inhaled droplet
119 size. Instillation leads to non-uniform, patchy deposition, primarily near the site of
120 instillation, and little or no alveolar deposition (37). Furthermore, inhalation methods are
121 preferable to injection as the aerosol is delivered directly to the site of infection, the
122 lungs, and hence is available there at higher concentrations (41). Semler et al. (42)
123 demonstrated that phage aerosol delivery by inhalation with a NOID was superior to
124 intraperitoneal delivery, as evidenced by a greater reduction in bacterial burden and
125 phage replication in the lungs.

126 Effective phage delivery to the lungs requires a prudent choice of aerosol delivery
127 device to avoid phage inactivation (27). Factors that may inactivate phage are described

128 elsewhere, and include shear stress, osmotic shock, and thermal stress, among others
129 (43,44). In a recent study, it was demonstrated that use of a vibrating mesh nebulizer
130 resulted in less phage D29 inactivation and a greater active phage D29 aerosol delivery
131 rate than use of a jet nebulizer (27). However, traditional NOID designs use jet
132 nebulizers and have very low delivery efficiency. An adequate delivery method that
133 allows retention of lytic capacity and ability to deliver high titers of phage are current
134 hurdles to testing prophylactic delivery of phages to the lungs of mice. In this study, a
135 NOID was modified for use with a vibrating mesh nebulizer to deliver high doses of
136 active phage D29 to the lungs of mice.

137 In order to advance phage D29 as a candidate therapy for TB, we leveraged our well-
138 established mouse model of low dose aerosol challenge of *Mtb*. We hypothesized that
139 sufficient prophylactic pulmonary delivery of phage D29 would reduce *Mtb* bacterial
140 burden 24 hours post-challenge. In order to evaluate our hypothesis, delivery
141 parameters maximizing the inhaled dose in a repeatable fashion were experimentally
142 simulated and subsequently used throughout the challenge studies. Measurements
143 were then performed to quantify the number of phage reaching the lungs of mice and
144 their clearance kinetics. Finally, phage D29 aerosol was delivered to mice prior to *Mtb*
145 aerosol challenge to evaluate prophylactic protection afforded by this treatment.

146 **Results**

147 **Lung Homogenization Does Not Reduce Phage Activity.** Naïve mouse lungs were
148 collected and spiked with an established titer of phage D29 and subsequently
149 homogenized to determine if this process, used routinely to evaluate *Mtb* CFU *ex vivo*,
150 would result in any loss of phage activity. The phage D29 titer after lung

151 homogenization was $12.08 \pm 0.03 \log_{10}(\text{PFU/mL})$ compared to the control titer before
 152 homogenization of $12.12 \pm 0.04 \log_{10}(\text{PFU/mL})$, with no significant difference ($p > 0.5$;
 153 $n=3$ each). These data indicate that the lung homogenization did not cause phage D29
 154 inactivation, nor did any innate tissue factor influence phage activity or the properties of
 155 the plaque assay used to quantify phage in a sample. This demonstrated the viability of
 156 this approach for quantifying pulmonary phage delivery.

157 **Nose-Only Inhalation Device - Dose Simulation Matches *In Vivo* Experiment.**

158 Tryptophan tracer deposition at different locations within two different versions of the
 159 NOID quantified by assay of rinsate are presented in Table 1, as is the predicted dose
 160 to the lungs of a mouse, $T_{m/A}$, calculated using equation {2} (see Materials and
 161 Methods). As shown, use of the smaller width of the first plenum achieved the target
 162 dose, with a $T_{m/A}$ of $1.0 \pm 0.1 \text{ PFU/alveolus}$, meaning that the total lung dose of active
 163 phage in the lungs of a mouse was predicted to be equal to the total number of alveoli in
 164 a mouse. The predicted dose of phage D29 to the lungs was 7.6 ± 0.1
 165 $\log_{10}(\text{PFU/mouse})$. Hence, this NOID configuration was chosen for *in vivo* experiments.

166 **Table 1.** Tryptophan tracer deposition within two different versions of the NOID as a
 167 simulation of phage D29 delivery.

First plenum width (mm)	Nebulizer reservoir (%)	First plenum (%)	Mixing tube (%)	Back plenum (%)	Nosepiece & adapter (%)	Mouse filter (%)	Exit filter (%)	Unaccounted (%)	Predicted dose to a mouse $T_{m/A}$ (PFU/alveolus)
95	1.0 ± 0.8	61.2 ± 7.5	1.9	5.1 ± 1.2	0.062 ± 0.008	0.013 ± 0.005	1.07 ± 0.05	30 ± 6	0.4 ± 0.2
32	1.2 ± 0.6	60.3 ± 0.4	3.2	6.3 ± 0.6	0.073 ± 0.004	0.033 ± 0.004	1.50 ± 0.023	27 ± 3	1.0 ± 0.1

Results are presented as avg \pm SD from 3 replicate experiments, except for the mixing tube which was measured once. The components are labeled in Figure 5 (Materials and Methods).

168 It is important to note that the ratio of flow rate entering the exit filter (478 mL/min) to the
169 flow rate entering the mouse filter and nosepiece with adapter (22 mL/min) was 22,
170 whereas the ratio of dose on the exit filter (1.50%) to dose on the surrogate mouse filter
171 and nosepiece with adapter (0.11%) was 14. If a uniform aerosol concentration were
172 present the ratios would be equal. The latter ratio was lower, as expected, due to
173 aerosol deposition in the front plenum.

174 A fraction of $0.044 = (22 \text{ mL/min}) / (500 \text{ mL/min})$ of the total dose reaching all 12
175 noseports deposited on the single tested mouse filter and nosepiece with adapter, on
176 which a dose of 0.11% was measured. Relative to the use of the unmodified NOID
177 presented by Nadithe et al. (36), the amount of tryptophan reaching the mouse filter was
178 improved by a factor of 1.8. Considering that approximately 6,000 times more active
179 phage D29 were delivered per unit time with the vibrating mesh nebulizer than with the
180 jet nebulizer (27), an improvement by a factor of approximately 11,000 was achieved
181 over the unmodified NOID that used a jet nebulizer, in terms of the predicted number of
182 active phage D29 reaching the lungs of the mice per unit time. The small standard
183 deviation indicated that the dosing was repeatable and consistent, and provided
184 confidence in this modified NOID setup.

185 We next optimized phage D29 aerosol delivery to mice in the modified NOID setup with
186 parameters described above. As phage D29 was amplified in *Mycobacterium*
187 *smegmatis*, the resulting lysate input to the nebulizer clogged the mesh and hence had
188 to be diluted 1:1 in isotonic saline prior to delivery, i.e. 3 mL of lysate at 11.8 ± 0.1
189 $\log_{10}(\text{PFU/mL})$ was added to 3 mL of isotonic saline and a combined total of 6 mL was
190 delivered. This resulted in lower delivery than the 6 mL of $12.2 \pm 0.1 \log_{10}(\text{PFU/mL})$

191 which was assumed during dose simulation. For the lower delivery conditions, the
 192 predicted dose in the lungs of mice was $6.9 \pm 0.1 \log_{10}(\text{PFU}/\text{mouse})$, which is within the
 193 range of doses measured *in vivo* in the lungs of mice after phage D29 aerosol delivery,
 194 shown in Table 2. This indicates that the method of dose simulation and the model
 195 given by equation {2} were accurate for predicting *in vivo* phage dose to the lungs of
 196 mice. This also demonstrates the accuracy and reliability of the dose simulation and the
 197 NOID setup in general.

198 **Table 2.** Phage D29 dose in the lungs of mice post-NOID delivery.

Time between exposure and euthanasia (min)	Phage D29 dose in mouse lungs in $\log_{10}(\text{PFU}/\text{mouse})^*$
0	6.6 ± 0.3
30	7.3 ± 0.1
90	7.0 ± 0.4

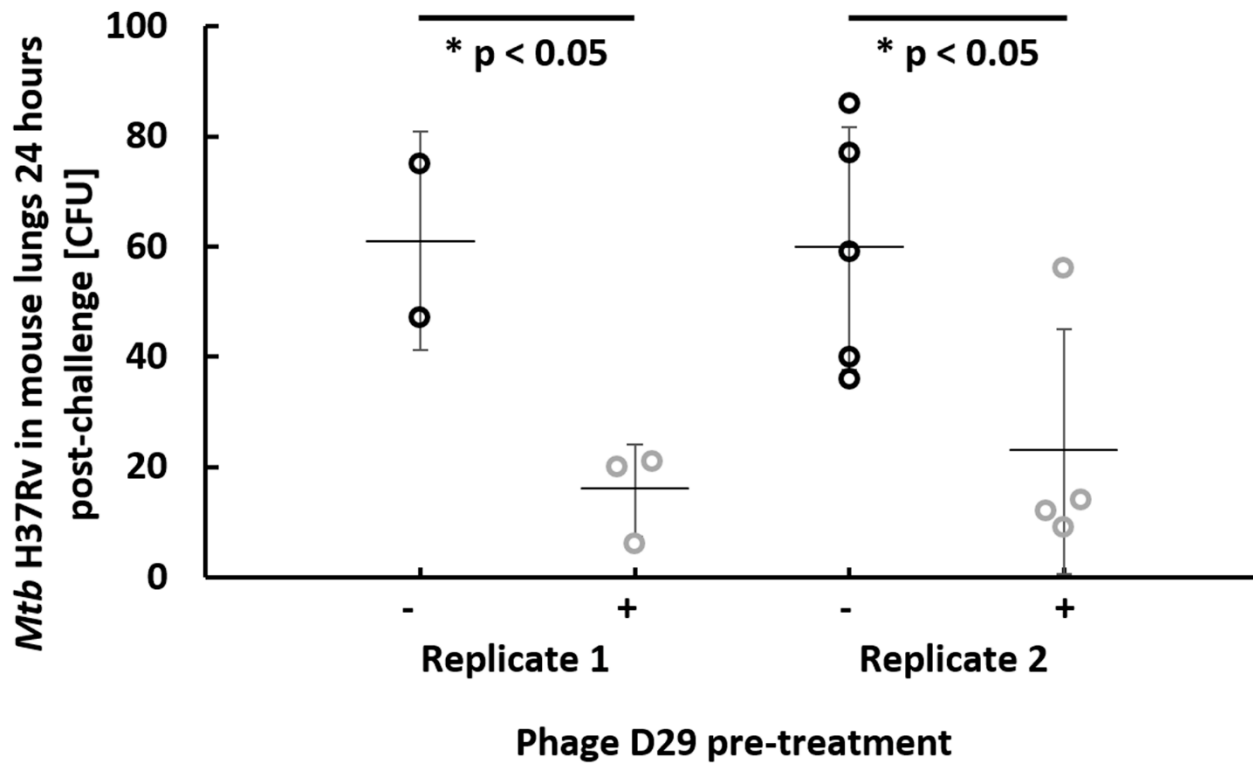
*avg \pm SD of n=3 mice per time point

199 Along with total immediate delivery, potential pulmonary clearance of phage D29 was
 200 evaluated 30 and 90 minutes post-delivery (see Table 2), and no statistically significant
 201 difference was observed ($p > 0.05$). Hence, phage D29 was not quickly cleared from the
 202 lungs of mice, providing confidence to proceed with *Mtb* exposure.

203 ***Mtb* H37Rv is Susceptible to Phage D29.** Before commencing bacterial aerosol
 204 challenge studies we confirmed prior data (45) indicating that *Mtb* strain H37Rv, a
 205 common laboratory strain, was susceptible to phage D29 lysate *in vitro*. A control plate
 206 (no phage added) contained 38 CFU, whereas 2 replicates with D29 addition resulted in

207 1 CFU and 2 CFU. Therefore, H37Rv lysis via phage D29 was 92-95% effective. The
208 lysis may have not been 100% effective due to phage not coming into contact with
209 every bacterium during plating, or potentially due to phage resistance. The high lysis
210 effectiveness provided confidence to proceed with *Mtb* exposure.

211 **Inhaled Phage D29 Provides *In Vivo* Prophylactic Protection against TB.** In order to
212 evaluate the potential application of phage D29 aerosol as a prophylactic tool against
213 *Mtb* infection we next quantified bacterial burden (CFU) of *Mtb* H37Rv in mouse lungs
214 24 hours post-infection, with or without phage D29 pre-treatment less than 30 minutes
215 prior to *Mtb* exposure. An average of $7.7 \pm 0.3 \log_{10}(\text{PFU/mouse})$ of phage D29 was
216 delivered to the lungs in replicate 2, which corresponded to ~1 PFU/alveolus on
217 average, indicating the target dose of phage D29 was achieved. A significant reduction
218 ($p < 0.05$) of bacterial burden in the lungs at 24 hours post-challenge was observed
219 (Figure 2). These data suggest that with a target dose of 1 PFU/alveolus, a significant
220 level of prophylactic protection against inhaled *Mtb* aerosol is indeed possible.



221

222 **Figure 2.** Pre-treatment with phage D29 aerosol delivered by nose-only inhalation

223 significantly reduces pulmonary bacterial burden 24 hours post-challenge with low dose

224 *Mtb* H37Rv. On the x-axis, “-” indicates no phage D29 pre-treatment and “+” indicates

225 phage D29 pre-treatment. Each circle represents a single mouse and error bars span

226 the standard deviation around the mean indicated by the horizontal line.

227 A separate cohort of mice from replicate 1 were followed out to 3 weeks post-challenge

228 to determine if effects of prophylactic phage application would persist over time.

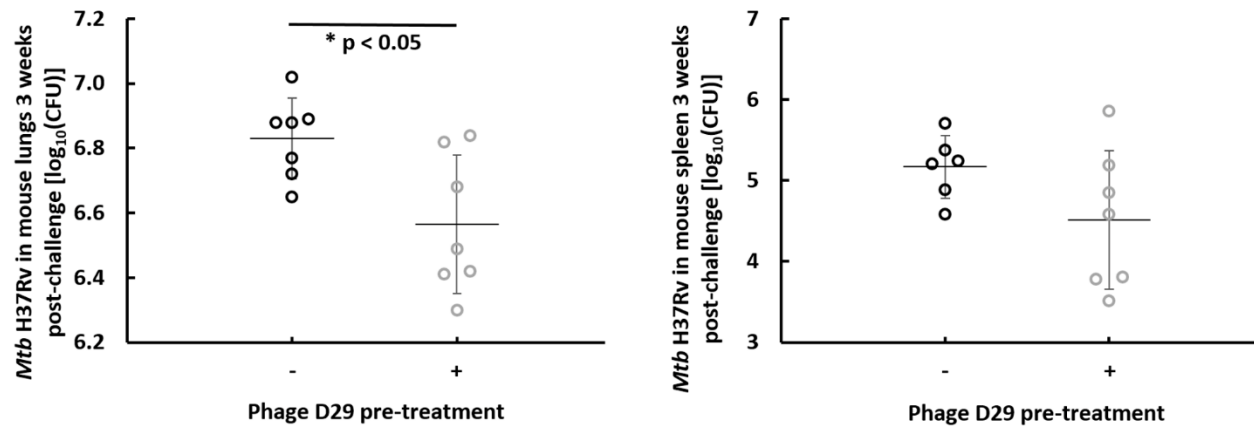
229 Bacterial burden was measured in the lungs and the spleen 3 weeks post-challenge

230 (Figure 3). Interestingly, at 3 weeks phage D29 pre-treated mice sustained a

231 significantly lower bacterial burden than mice that did not receive phage pre-treatment

232 in the lungs ($p < 0.05$), although bacterial burden was not significantly different in the

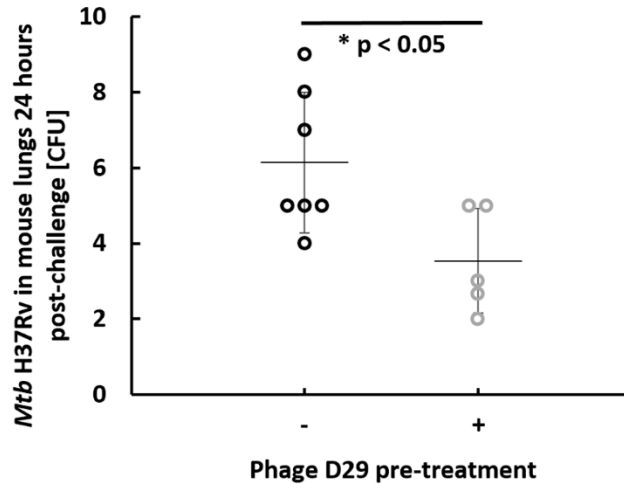
233 spleen ($p > 0.1$). The bacterial burden at 3 weeks was of a high magnitude.



234

235 **Figure 3.** Log₁₀ of bacterial burden 3 weeks post-challenge in the lungs (left) and spleen
 236 (right), without and with phage D29 pre-treatment. On the x-axis, “-” indicates no phage
 237 D29 pre-treatment and “+” indicates phage D29 pre-treatment. Each circle represents a
 238 single mouse and error bars span the standard deviation around the mean indicated by
 239 the horizontal line.

240 In order to more closely simulate *Mtb* infections in humans we next optimized and
 241 utilized an ultra-low dose aerosol challenge of H37Rv calibrated to deliver 5-10 CFU of
 242 bacteria. An average of 7.4 ± 0.1 log₁₀(PFU/mouse) of phage D29 was delivered to the
 243 lungs. At 24 hours post-challenge, a significant reduction ($p < 0.05$) of *Mtb* in the lungs
 244 was observed in the group that received phage D29 aerosol pre-treatment, relative to
 245 the group that did not (Figure 4), providing important further evidence of prophylactic
 246 efficacy.



247

248 **Figure 4.** Pre-treatment with phage D29 aerosol delivered by nose-only inhalation
 249 significantly reduces pulmonary bacterial burden 24 hours post-challenge with ultra-low
 250 dose *Mtb* H37Rv. On the x-axis, “-” indicates no phage D29 pre-treatment and “+”
 251 indicates phage D29 pre-treatment. Each circle represents a single mouse and error
 252 bars span the standard deviation around the mean indicated by the horizontal line.

253 **Discussion**

254 The results of this study demonstrate that inhalation of phage D29 aerosol prior to
 255 challenge with *Mtb* aerosol can significantly decrease the pulmonary bacterial burden in
 256 mice 24 hours post-infection. These data suggest that inhaled mycobacteriophage
 257 aerosol resulted in *Mtb* lysis in the lungs prior to macrophage uptake and granuloma
 258 formation. This proof-of-principle study may have implications for the development of
 259 prophylactic aerosol treatments for health care professionals exposed to patients with
 260 active TB and reduction in *Mtb* transmission rates in this setting. This is important
 261 because many health care professionals are relatively unwilling to work in areas of
 262 hospitals with high-risk of tuberculosis transmission (46). Additionally, more protection
 263 could potentially be offered to individuals in areas in which TB is endemic, or to other

264 individuals at high-risk, such as household contacts and visiting family members at
265 hospitals. This treatment is intended to complement normal precautions, which includes
266 use of administrative controls, environmental controls, and personal respiratory
267 protection (13,14).

268 The authors are only aware of one other study regarding prophylactic inhalation of
269 phages prior to inhalation of bacteria (47), and that study demonstrated 4-day
270 prophylaxis against multi-drug-resistant (MDR) *Pseudomonas aeruginosa* in mice, but
271 used intranasal instillation rather than an aerosol delivery device. Instillation results in
272 localized deposition and is not as representative of natural inhalation to the different
273 regions of the lungs as nose-only inhalation (37,48). Therefore, we believe this work,
274 the first study demonstrating prophylactic protection with phage using nose-only
275 inhalation of aerosol, represents a significant advancement in this area of research.
276 Additionally, to the authors' knowledge, a much higher titer of phage was delivered to
277 the lungs of mice by nose-only inhalation in this study than in any previous study.
278 Relative to the use of a jet nebulizer in a previous NOID design (36), approximately
279 11,000 times more active phage D29 could be delivered to the lungs of mice, and with
280 repeatable results, indicating a major improvement of dosing to mice was achieved with
281 this novel approach. Furthermore, Liu et al. (41) only delivered 10^2 – 10^3 PFU of phage
282 D29 to the lungs of mice using a Collison jet nebulizer with a NOID, which is orders of
283 magnitude lower than in this study, in which $> 10^7$ PFU was delivered to the lungs of
284 mice. This improvement allowed, for the first time, an average dose of ~ 1 PFU/alveolus
285 to be achieved. It is important to consider that some alveoli are poorly perfused, and
286 hence > 1 PFU per accessible alveolus may have been achieved on average. Another

287 factor to consider is that phage progeny released after *Mtb* lysis would offer further
288 protection in their vicinity, but are unlikely to be transferred to nearby alveoli, as they are
289 non-motile. As *Mtb* is also non-motile, it is unlikely to move between alveoli and come
290 into contact with phage in that manner prior to uptake by immune cells.

291 The prophylactic delivery of a calculated average of 1 PFU/alveolus allowed for a
292 significant reduction of *Mtb* levels in the lungs, demonstrating a prophylactic effect.
293 Whether such a decrease in *Mtb* levels is sufficient to decrease mortality rates is not
294 known. While it is difficult to deliver more than 1 PFU/alveolus on average to a mouse
295 using a NOID, such levels may be necessary to achieve complete bacterial eradication.
296 Poisson statistics can be used to estimate the probability of a specific random
297 occurrence during an interval of interest knowing the average number of occurrences in
298 that interval (49). Using this method, the probability, P , that an alveolus will contain a
299 certain number of phage, x , can be predicted knowing the average number of
300 PFU/alveolus, λ , according to

$$P = \frac{e^{-\lambda} \cdot \lambda^x}{x!} \quad \{1\}$$

301 Using the values $\lambda = 1$ and $x = 0$ gives $P = 0.37$. This indicates that if on average 1
302 PFU/alveolus is delivered to the lungs, the probability that an alveolus does not contain
303 a phage is still 37%. Hence, the chance that a bacterium encounters at least one phage
304 in an alveolus is about 63%. In prophylactic phage administration experiments (see
305 Figure 2) the average reduction in bacterial burden was from approximately 60 CFU to
306 approximately 20 CFU, or about 67%. This is in close agreement with the theoretically

307 calculated prediction of 63% reduction in bacterial burden that assumes that all bacteria
308 that deposit in an alveolus in the presence of at least one phage are inactivated.

309 To achieve at least one phage in 99% of the alveoli of a mouse, the average number of
310 phage per alveolus would need to be $\lambda = 4.6$. For 99.9% coverage, it is $\lambda = 6.9$. A
311 potential indicator of the dose required for complete prophylaxis is when the probability
312 that an alveolus contains no phage becomes less than the inverse of the number of
313 alveoli in the lungs, which for a mouse occurs with $\lambda > 17.5$.

314 Achieving a high dose of active phage in human lungs is not as difficult as in mice
315 because deposition losses in the NOID would not be present and humans do not
316 require equally small droplets for efficient lung deposition. Human lungs contain
317 $\sim 4.8 \times 10^8$ alveoli (50), ~ 10 times the number that mouse lungs have. An average
318 number of phage per alveolus of approximately 20 may be required for complete
319 prophylaxis in a human according to the above indicator. A recent study suggested that
320 in humans, a respirable dose of active phage D29 of $\sim 1.3 \times 10^9$ PFU could be achieved
321 with delivery of 6 mL of diluted lysate using a vibrating mesh nebulizer (27). This
322 corresponds to a dose to human lungs of ~ 2.7 PFU/alveolus on average, or 93%
323 alveolar coverage. In that study, the phage D29 lysate was diluted 1:100 in isotonic
324 saline prior to aerosolization as without dilution the lysate purification level was not
325 sufficient to prevent mesh clogging. Potentially, without dilution, i.e. with better
326 purification techniques, orders of magnitude higher titers may reach the lungs, on the
327 order of 10^2 PFU/alveolus on average. This could be sufficient for complete prophylaxis
328 according to the above described Poisson statistics argument. The chance of non-
329 contact between phage and bacteria would be substantially decreased at this dose

330 level. Additionally, with daily prophylactic doses, the likelihood that a specific alveolus
331 receives a sufficient number of phages to eradicate intruding bacteria increases. As it
332 may take days for granulomas to form (51), it is possible that phages delivered soon
333 after *Mtb* exposure may still offer protection, but this depends on macrophage uptake
334 dynamics (33), and awaits further exploration.

335 The development of regulatory-approved, commercial phage formulations for inhalation
336 will likely require the use of cocktails containing various phages that target different
337 receptors to ensure the *Mtb* does not become phage-resistant (17). The development of
338 anti-TB cocktails is an active area of research (17). Phage D29 and others that may be
339 included in a therapeutic cocktail would be applicable for prevention of drug-sensitive or
340 drug-resistant strains of *Mtb*. Further development of phage cocktail therapy will require
341 efficacy testing against clinical and drug-resistant *Mtb* strains and, importantly,
342 measuring potential phage-induced host immune responses. It should be determined
343 whether daily prophylactic doses of phage cocktails lead to an immune response that
344 inactivates the phages, or to the development of bacteria which are resistant to all of the
345 phages in the cocktail, although it is important to note that phages are capable of
346 mutating to overcome bacterial resistance and new phages targeting different receptors
347 can be isolated relatively rapidly. Some clinical applications of phage therapy have
348 reported humoral immune responses to phage (anti-phage IgG and IgM antibodies),
349 however the magnitude of the anti-phage antibody response did not correlate with a
350 decrease in clinical efficacy (52). This suggests that even if an adaptive immune
351 response to phage is induced it may not be detrimental to the host nor inhibit phage
352 efficacy. Although recent evidence suggests that mucosal delivery (aerosol) does not

353 induce a robust or detrimental anti-phage immune response (53), future work should
354 specifically examine the effects of repeated phage exposure to determine feasibility of
355 protection in high risk populations likely to regularly encounter *Mtb*.

356 In therapeutic TB treatment, for example, with antibiotics, drug-resistant *Mtb* persisters
357 may arise if not all bacteria are eradicated (54). Persisters may arise to some extent in
358 prophylaxis using phages if there are bacteria that are less likely to be lysed by phages
359 and hence have a higher probability to establish an infection. However, therapeutic
360 treatment typically requires eradicating a large population in which a small proportion
361 may be resistant, whereas prophylactic treatment typically requires eradicating a much
362 smaller population, perhaps even as low as a single bacterium. Therefore, the
363 probability of establishing resistant *Mtb* is expected to be smaller for prophylaxis as
364 compared to therapy.

365 For future development of phage cocktails it will be important to ensure that each type
366 of phage is capable of surviving the nebulization process and can effectively reach the
367 lungs. In this study, experimental dose simulation of phage delivery to mice using a
368 tryptophan tracer, simulated breathing, and filter aerosol capture with a NOID, resulted
369 in accurate prediction of phage dose reaching the lungs of mice *in vivo*. Hence,
370 assuming the same droplet size distribution, it is possible that one could simply
371 measure the phage activity retention from the nebulizer by aerosolization to a filter as
372 described elsewhere (27), and predict the *in vivo* dose reaching the lungs of mice in the
373 present NOID setup using the modelling approach (see equation {2}) and aerosol
374 delivery efficiency results (Table 1) presented in this study. This would allow the lung
375 dose of different phages in a cocktail to be predicted prior to *in vivo* experiments, saving

376 time and resources, reducing the risk of failed animal work, and expediting the
377 development process.

378 In summary, inhalation of anti-TB mycobacteriophage D29 aerosol is a promising and
379 novel approach to provide prophylactic protection against primary infection of inhaled
380 *Mtb* aerosol. Significant reduction in bacterial burden was achieved with prophylactic
381 delivery of an average dose of active phage D29 of ~1 PFU/alveolus to the lungs.
382 Complete prophylaxis may be achievable with larger or repeated doses of active
383 phages. The number of active phages reaching the alveoli can be predicted prior to
384 animal studies with a NOID by aerosolizing a tracer, simulating breathing through a
385 filter, assay of the recovered aerosol on the filter, and applying the developed
386 mathematical modeling approach. The development of a high titer phage cocktail
387 against TB is recommended over monophage therapy. The cocktail may provide extra
388 protection to health care professionals regularly exposed to patients with active TB and
389 to individuals in areas with high rates of TB transmission whilst limiting the likelihood of
390 resistance to phages. Additionally, countries with a high burden of TB and MDR-TB are
391 often involved in military engagement with resulting additional risk of exposure. Given
392 that the risk of *Mtb* transmission is higher in congregate settings, a single individual with
393 TB disease exerts an immediate and disruptive impact upon patients' lives, military
394 operations, and daily functioning at military and civil treatment facilities. Delivery of high
395 doses of active phages to human lungs for prophylactic purposes appears achievable
396 and proceeding to human clinical trials is of interest and compliance to delivery of high
397 doses of phage aerosol on a daily basis should be studied.

398 **Materials and Methods**

399 **Mice.** The mice used in this study were female C57BL/6 mice 4-6 weeks of age,
400 weighing 14-16 grams, purchased from Charles River Laboratories (Wilmington, MA,
401 USA). Mice were housed at the Infectious Disease Research Institute (IDRI) biosafety
402 level 3 animal facility under pathogen-free conditions and were handled in accordance
403 with the specific guidelines of IDRI's Institutional Animal Care and Use Committee. The
404 reported minute ventilation rate for CD-1 mice, similar to the C57BL/6 strain used here,
405 was 1.46 mL/gram of body weight (55). For an average mass of 15 grams, this
406 corresponds to an average minute ventilation of ~22 mL/min per mouse, and this value
407 was used for calculations for nose-only aerosol delivery.

408 **Phage D29 Amplification, Shipping, and Plaque Assay.** Phage D29 was prepared to
409 a titer of 1.6×10^{12} PFU/mL via replication with *M. smegmatis* strain mc²155 using solid
410 media, sterile filtration, centrifugation, and pellet resuspension in buffer, as described
411 elsewhere (<https://phagesdb.org/workflow/>, 27). The amplified phage lysate was
412 shipped to IDRI (Seattle, WA, USA) from the University of Alberta (Edmonton, AB,
413 Canada) using cold packs and a Styrofoam container. This shipment did not result in
414 titer reduction of the lysate. The titer of phage D29 was measured using full-plate
415 plaque assay, as described elsewhere (<https://phagesdb.org/workflow/>, 27).

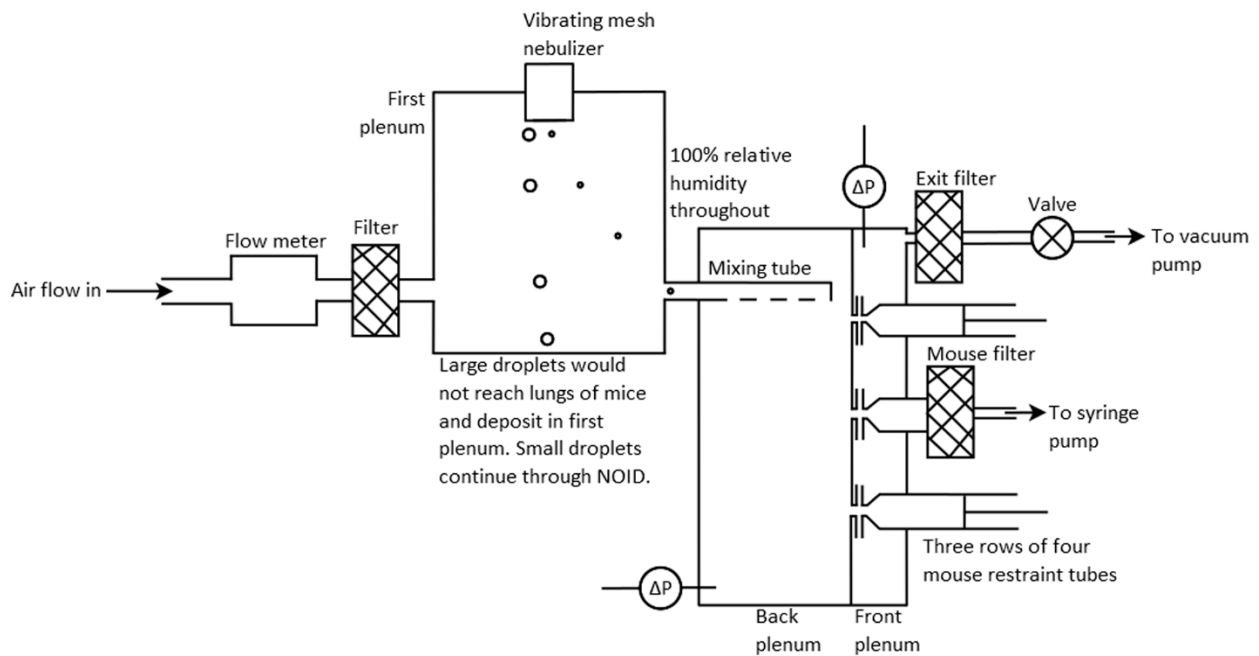
416 **Lung Homogenization.** It was necessary to homogenize the lungs of the mice to
417 generate a representative liquid sample to assay and to determine the number of active
418 phage and bacterial burden in the lungs. To verify the phage remained active after the
419 high-shear homogenization process, a 20- μ L sample of phage lysate was spiked in lung
420 tissue within 2 mL of buffer, in a 15-mL Eppendorf tube, homogenized (Omni Prep Multi-
421 Sample Homogenizer, Omni International; Kennesaw, GA, USA) for 1 minute, and

422 centrifuged for 2 minutes at 1800 rpm. The titer after homogenization was compared to
423 the titer before homogenization to determine if the homogenization process inactivated
424 the phages.

425 **Nose-Only Inhalation Device – Device Design and Dose Simulation vs. *In Vivo***

426 **Experiment.** A schematic of the developed NOID, a modified version of the device
427 described by Nadithe et al. (36), set up for dose simulation experiments, is shown in
428 Figure 5. Nadithe et al. (36) reported that their NOID design had substantial losses of
429 aerosol. Only $0.108 \pm 0.027\%$ of the dose input to the jet nebulizer reached the mice,
430 and only $8.19 \pm 3.56\%$ of that amount reached the lungs of the mice. This corresponded
431 to $0.0087 \pm 0.0021\%$ (870 ppm) of the input dose reaching the lungs of all 12 mice
432 combined. Much of this loss was attributed to the compressor of the jet nebulizer
433 delivering 4.5 L/min of air flow into the system, resulting in a substantial amount of
434 aerosol convecting by the noses of the mice and exiting the back of the device unused.
435 This is because the combined total minute volume for 12 mice is only 0.264 L/min, and
436 hence about 4.2 L/min of air flow, or 93% of aerosol available at the nosepieces,
437 bypassed the mice. Therefore, in our modified design the minimum air flow rate into the
438 system that could safely be used without developing a hypoxic environment (38), i.e. 0.5
439 L/min, was used. The negative pressure induced by a vacuum pump (Model
440 UN726FTP, KNF Neuberger, Inc.; Trenton, NJ, USA) past the exit of the device caused
441 the air flow into the NOID. The pressure difference between the front plenum, back
442 plenum, and atmosphere was measured with manometers to rule out leaks in the
443 system. A rotameter (Catalogue No. 5079K63; McMaster-Carr, Elmhurst, IL, USA),
444 calibrated with a thermal mass flow meter (TSI 4043; TSI Incorporated, Shoreview, MN,

445 USA), was used to measure the air flow rate into the NOID, which was controlled with
 446 valves past the exit filter and in the rotameter. An inlet air filter (Respirgard II 303; Vital
 447 Signs Incorporated, Englewood, CO, USA) prevented foreign virus or bacterial
 448 contamination from the air flow into the device.



449
 450 **Figure 5.** Schematic of a modified NOID adapted for use with a vibrating mesh
 451 nebulizer.

452 The NOID was modified to incorporate a vibrating mesh nebulizer (Aerogen Solo with
 453 Pro-X Controller; Aerogen Ltd., Dangan, Galway, Ireland) to produce the aerosol. The
 454 aerosol entered the first plenum, which was developed as preliminary experiments
 455 demonstrated that use of the commercial wye connector for the vibrating mesh
 456 nebulizer resulted in a large extent of aerosol recirculation, droplet coalescence, and
 457 deposition losses. This is because the small-volume wye connector was designed for
 458 use of > 3 L/min air flow rate whereas a lower air flow rate, 0.5 L/min, was used in this
 459 study.

460 The operation of the vibrating mesh nebulizer has been described by Carrigy et al. (27).
461 The mesh consists of ~1000 orifices, each with a diameter of ~3 μm . The generated
462 aerosol has been measured at the exit of a T-piece by laser diffraction to have a volume
463 median diameter of ~5.5 μm and geometric standard deviation of ~1.8 (56). The
464 vibrating mesh nebulizer has a liquid droplet production rate of about 0.36 mL/min (27),
465 and hence with the chosen air flow in of 500 mL/min, liquid entered the system at a
466 concentration of 720 g/m³. Considering that room temperature air can hold ~17.3 g/m³,
467 the nebulizer produces approximately 42 times the amount of liquid required to fully
468 saturate the air flow in, assuming it is initially dry. Hence, at a maximum, only about 2%
469 of the mass of the droplets, corresponding to about 1% of the diameter assuming
470 sphericity, is required to fully saturate the NOID. Therefore, the droplets essentially
471 maintained their size after atomization as they transited through the device, neglecting
472 any coalescence. However, mice require small droplets for deposition in the lungs
473 (36,57). In the present NOID system, the large droplets were filtered out by the first
474 plenum and the smaller droplets produced by the nebulizer, recalling that the geometric
475 standard deviation is ~2, followed the air flow streamlines, due to a lower Stokes
476 number, into the ~12-mm diameter mixing tube. This mixing tube ensured a uniform
477 aerosol concentration entered near the top of the back plenum. Mice inhale through
478 nosepieces attached to mouse restraint tubes, which used an airtight plunger to hold the
479 mice in place with their noses at the noseports. The mice inhaled the aerosol from the
480 back plenum through the noseports, and the excess air flow and exhaled air from the
481 mice entered the front plenum and subsequently were filtered and exited the device.

482 Before proceeding to *in vivo* experiments, the dose was simulated to verify a
483 biologically-relevant amount of aerosol would reach the lungs of mice. For dose
484 simulation experiments a mouse restraint tube was replaced with a filter and attached to
485 the nosepiece by an adapter, rapid-prototyped out of an acrylic compound (Objet
486 VeroGray RGD850; Eden Prairie, MN, USA) using a PolyJet 3D printer (Objet Eden 350
487 V High Resolution 3D Printer, Stratsys, Ltd.; Eden Prairie, MN, USA). This filter was
488 termed a mouse filter due to its surrogate mouse function and location within the set-up
489 and was attached to a syringe pump (PHD ULTRA Syringe Pump with Push/Pull
490 Mechanism; Model no. 70-3008; Harvard Apparatus, Holliston MA, USA). The syringe
491 pump initiated a constant flow rate of 22 mL/min through the mouse filter, which is
492 equivalent to the average minute volume for a mouse, as described previously. Only
493 one port was evaluated because previous data with the unmodified NOID demonstrated
494 a reasonably even distribution of aerosol between noseports (36). Due to the > 10 mL
495 filter dead volume, the steady flow equivalent of tidal flow was used, and the effect of
496 exhalation on lung deposition was neglected. L-Tryptophan (Cat #93659; Sigma Aldrich,
497 St. Louis, MO, USA) tracer in isotonic saline was atomized and captured on the mouse
498 filter, as well as at various points within the NOID (nebulizer reservoir, first plenum,
499 mixing tube, back plenum, nosepiece and adapter, exit filter) to determine where
500 deposition occurred. The tracer concentration was assayed using ultraviolet-visible (UV-
501 Vis) spectrophotometry (8452A Diode Array Spectrophotometer; Hewlett-Packard,
502 Mississauga, ON, Canada). The deposition was quantified for two different versions,
503 where different widths of the developed first plenum were tested: 32 mm and 95 mm.
504 The length of the first plenum was kept fixed at 152 mm and the depth was kept fixed at

505 211 mm, as this was approximately the distance at which bulk aerosol flow emitted from
506 the nebulizer stopped after horizontal spray. Three replicate dose simulation
507 experiments were performed for each of the two first plenum widths. As the interior
508 volume of the NOID was ~4 L, the air flow through the system was allowed to continue
509 for ~8 minutes after nebulization was complete to allow time for the aerosol to transit
510 through the system.

511 A model was developed to predict the average number of active phage per alveolus
512 reaching the lungs of one mouse in the NOID, $T_{m/A}$, from the tryptophan experiments
513 and literature data, and is given by,

$$T_{m/A} = \frac{T_0 \cdot f_n \cdot f_i \cdot f_m \cdot f_l}{A_m} \quad \{2\}$$

514 where T_0 is the initial titer of the lysate input into the vibrating mesh nebulizer in PFU, f_n
515 is the fraction of the phage not inactivated by the nebulizer measured in a previous
516 study to be 0.319 (27), f_i is the fraction of the breathing cycle spent inhaling
517 approximated as 0.5, f_m is the fraction of the aerosol emitted from the nebulizer that is
518 inhaled by a single mouse from tryptophan tracer dose simulation experiments, f_l is the
519 fraction of aerosol that is inhaled by a mouse that reaches its lungs taken as 0.08 (36),
520 and A_m is the number of alveoli per mouse taken as 4×10^7 (58).

521 For comparison to dose simulation, phage D29 was delivered to mice and the lungs of
522 the mice were removed following euthanasia and homogenized within 5 mL of buffer.
523 The number of active phage in the homogenate was determined by plaque assay.

524 Three mice were taken down at each of 0, 30, and 90 minutes after phage exposure to
525 obtain a preliminary measure of lung clearance.

526 **Host Susceptibility.** Prior to performing *in vivo* experiments it was confirmed that *Mtb*
527 H37Rv is susceptible to phage D29 lysis. A volume of 100 μ L of 10^{11} PFU/mL of phage
528 D29 lysate was added to a sample of *Mtb* H37Rv and subsequently plated on agar
529 plates. Bacterial CFU was determined after incubating plates at 37°C and 5% CO₂ for
530 21 days. Plates with or without D29 application were compared.

531 ***In Vivo* Prophylactic Protection.** The mice were acclimatized to remain calm in the
532 restraint tubes of the NOID as per previous methods (57), therefore retaining a normal
533 breathing pattern to maximize peripheral lung deposition. Briefly, mice were ‘trained’ in
534 the NOID tubes without treatment 3-5 times for 5 minutes each in the week leading up
535 to phage delivery. This training significantly reduced visible stress-induced changes in
536 breathing. Within 30 minutes of receiving phage D29 aerosol with the NOID, mice were
537 challenged with *Mtb* H37Rv aerosol using a previously described Wisconsin-Madison
538 aerosol chamber (6,59), calibrated to deliver ~50-100 bacteria (low dose) or ~5-10
539 bacteria (ultra-low dose). The dose nomenclature was based on previous studies (6,60-
540 62). After *Mtb* aerosol inhalation and euthanasia, the lung tissue was isolated and
541 homogenized in 5 mL of PBS + Tween-80 (Sigma-Aldrich, St. Louis, Missouri, USA)
542 buffer and the entire lung homogenate sample was plated on Middlebrook 7H10 agar
543 plates and subsequently incubated at 37°C and 5% CO₂ for 3 weeks before colonies
544 were counted. The bacterial burden of *Mtb* was evaluated 24 hours (n=2 experiments)
545 and 21 days (n=1 experiment) post-challenge for the low dose model and at 24 hours
546 (n=1 experiment) for the ultra-low dose model. The ultra-low dose bacterial challenge is

547 expected to better reflect human infection conditions where relatively few bacteria are
548 able to establish a pulmonary infection in the host. The NOID was disassembled and
549 components were disinfected with ethanol between all experiments. Following aerosol
550 challenge with *Mtb* H37Rv, the Wisconsin-Madison aerosol chamber was thoroughly
551 sprayed with Lysol aerosol and after 10 minutes cleaned with 70% ethanol and paper
552 towels. Nebulizer components were sterilized between runs with 10% bleach.

553 **Statistics.** Significance was evaluated using Student's t-tests assuming equal variance
554 at a significance level of 0.05. Two-sided t-tests were used to determine if results were
555 significantly different, and one-sided t-tests were used to determine whether a result
556 was significantly greater than or less than another result. Experimental results are
557 generally represented as mean \pm standard deviation.

558 **Acknowledgements**

559 NC thanks the Killam Trusts, the Natural Sciences and Engineering Research Council
560 of Canada, Alberta Innovates, and the University of Alberta for scholarship funding. NC
561 thanks Bernie Faulkner for manufacturing the first plenum. The vibrating mesh nebulizer
562 equipment was kindly provided by Jim Fink and Ronan MacLoughlin (Aerogen Ltd.).
563 The funders and equipment providers had no role in study design, data collection and
564 interpretation, or the decision to submit the work for publication. Research reported in
565 this publication was supported by the National Institute of Allergy and Infectious
566 Diseases of the National Institutes of Health under award number R01AI125160 and
567 SEL is supported through the University of Washington Diseases of Public Health
568 Importance T32 training grant number A1075090. The content is solely the

569 responsibility of the authors and does not necessarily represent the official views of the
570 National Institutes of Health.

571 **References**

572 1. World Health Organization. 2018. Global tuberculosis report 2018. Available from:
573 https://www.who.int/tb/publications/global_report/en/

574 2. Orr P. 2013. Tuberculosis in Nunavut: looking back, moving forward. CMAJ 185:287-
575 288.

576 3. Contreras GL, Awashthi S, Hanif SNM, Hickey AJ. 2012. Inhaled vaccines for the
577 prevention of tuberculosis. J Mycobac Dis S:1.

578 4. Tyne AS, Chan JGY, Shanahan ER, Atmosukarto I, Chan H-K, Britton WJ, West NP.
579 2013. TLR2-targeted secreted proteins from *Mycobacterium tuberculosis* are protective
580 as powdered pulmonary vaccines. Vaccine 31:4322-4329.

581 5. Aerosol Vaccines for Tuberculosis Workshop Summary Group. 2015. Developing
582 aerosol vaccines for *Mycobacterium tuberculosis*: workshop proceedings National
583 Institute of Allergy and Infectious Diseases, Bethesda, Maryland, USA, April 9, 2014.
584 Vaccine 33:3038-3046.

585 6. Baldwin SL, Reese VA, Huang PD, Beebe EA, Podell BK, Reed SG, Coler RN. 2016.
586 Protection and long-lived immunity induced by the ID93/GLA-SE vaccine candidate
587 against a clinical *Mycobacterium tuberculosis* isolate. Clin Vaccine Immunol 53:137-
588 147.

- 589 7. Nemes H, Geldenhuys H, Rozot V, Rutkowski KT, Ratangee F, Bilek N, Mabwe S,
590 Makhethhe L, Erasmus M, Toefy A, Mulenga H, Hanekom WA, Self SG, Bekker L-G,
591 Ryall R, Gurunathan S, DiazGranados CA, Andersen P, Kromann I, Evans T, Ellis RD,
592 Landry B, Hokey DA, Hopkins R, Ginsberg AM, Scriba TJ, Hatherill M. 2018. Prevention
593 of *M. tuberculosis* infection with H4:IC31 vaccine or BCG revaccination. *N Engl J Med*
594 379:138-149.
- 595 8. Rodrigues LC, Mangtani P, Abubakar I. 2011. How does the level of BCG vaccine
596 protection against tuberculosis fall over time? *BMJ* 343:d5974.
- 597 9. Rowland R, McShane H. 2014. Current transmission prevention methods:
598 vaccination, p 33-52. *In* Zellweger J-P (ed), *Clinical insights: tuberculosis prevention*.
599 Future Medicine Ltd, London, UK.
- 600 10. Toujani S, Cherif J, Mjid M, Hedhli A, Ouahchy Y, Beji M. 2017. Evaluation of
601 tuberculin skin test positivity and early tuberculin conversion among medical intern
602 trainees in Tunisia. *Tanaffos* 16:149-456.
- 603 11. Joshi R, Reingold AL, Menzies D, Pai M. 2006. Tuberculosis among health-care
604 workers in low- and middle-income countries: a systematic review. *PLoS Med* 3:e494.
- 605 12. Uden L, Barber E, Ford N, Cooke GS. 2017. Risk of tuberculosis infection and
606 disease for health care workers: an updated meta-analysis. *Open Forum Infect Dis*
607 4:ofx137.
- 608 13. Fox GJ, Marks GB, Britton WJ. 2014. Current transmission prevention methods:
609 reducing disease spread from infected individuals, p 53-76. *In* Zellweger J-P (ed),
610 *Clinical insights: tuberculosis prevention*. Future Medicine Ltd, London, UK.

- 611 14. Verkuil S, Middelkoop K. 2016. Protecting our front-liners: occupational tuberculosis
612 prevention through infection control strategies. *Clin Infect Dis* 62:S231-S237.
- 613 15. Hatfull GF. 2015. Dark matter of the biosphere: the amazing world of bacteriophage
614 diversity. *J Virology* 89:8107-8110.
- 615 16. Loc-Carrillo C, Abedon ST. 2011. Pros and cons of phage therapy. *Bacteriophage*
616 1:111-114.
- 617 17. Hatfull GF, Vehring R. 2016. Respirable bacteriophage aerosols for the prevention
618 and treatment of tuberculosis, p 277-292. *In* Hickey AJ, Misra A, Fourie PB (ed), *Drug*
619 *delivery systems for tuberculosis prevention and treatment*. John Wiley & Sons, Ltd,
620 Chichester, UK.
- 621 18. Abedon ST, Kuhl SJ, Blasdel BG, Kutter EM. 2011. Phage treatment of human
622 infections. *Bacteriophage* 1:66-85.
- 623 19. Gordillo Altamirano FL, Barr JJ. 2019. Phage therapy in the postantibiotic era. *Clin*
624 *Microbiol Rev* 32:e00066-18.
- 625 20. Schooley RT, Biswas B, Gill JJ, Hernandez-Morales A, Lancaster J, Lessor L, Barr
626 JJ, Reed SL, Rohwer F, Benler S, Segall AM, Taplitz R, Smith DM, Kerr K,
627 Kumaraswamy M, Nizet V, Lin L, McCauley MD, Strathdee SA, Benson CA, Pope RK,
628 Leroux BM, Picel AC, Mateczun AJ, Cilwa KE, Regeimbal JM, Estrella LA, Wolfe DM,
629 Henry MS, Quinones JV, Salka S, Bishop-Lilly KA, Young R, Hamilton T. 2017.
630 Development and use of personalized bacteriophage-based therapeutic cocktails to
631 treat a patient with a disseminated resistant *Acinetobacter baumannii* infection.
632 *Antimicrob Agents Chemother* 61:e00954-17.

- 633 21. Dedrick RM, Guerrero-Bustamante CA, Garlena RA, Russell DA, Ford K, Harris K,
634 Gilmour KC, Soothill J, Jacobs-Sera D, Schooley RT, Hatfull GF, Spencer H.
635 Engineered bacteriophages for treatment of a patient with a disseminated drug resistant
636 *Mycobacterium abscessus*. Nat Med 25:730-733.
- 637 22. Abedon ST. 2015. Phage therapy of pulmonary infections. Bacteriophage 5:1-13.
- 638 23. Golshahi L, Seed KD, Dennis JJ, Finlay WH. 2008. Toward modern inhalational
639 bacteriophage therapy: nebulization of bacteriophages of *Burkholderia cepacia*
640 complex. J Aerosol Med Pulm Drug Deliv 21:351-360.
- 641 24. Golshahi L, Lynch KH, Dennis JJ, Finlay WH. 2011. *In vitro* lung delivery of
642 bacteriophages KS4-M and ϕ KZ using dry powder inhalers for treatment of *Burkholderia*
643 *cepacia* complex and *Pseudomonas aeruginosa* infections in cystic fibrosis. J Appl
644 Microbiol 110:106-117.
- 645 25. Matinkhoo S, Lynch KH, Dennis JJ, Finlay WH, Vehring R. 2011. Spray-dried
646 respirable powders containing bacteriophages for the treatment of pulmonary infections.
647 J Pharm Sci 100:5197-5205.
- 648 26. Hoe S, Boraey MA, Ivey JW, Finlay WH, Vehring R. 2014. Manufacturing and
649 device options for the delivery of biotherapeutics. J Aerosol Med Pulm Drug Deliv
650 27:315-328.
- 651 27. Carrigy NB, Chang RY, Leung SSY, Harrison M, Petrova Z, Pope WH, Hatfull GF,
652 Britton WJ, Chan H-K, Sauvageau D, Finlay WH, Vehring R. 2017. Anti-tuberculosis
653 bacteriophage D29 delivery with a vibrating mesh nebulizer, jet nebulizer, and soft mist
654 inhaler. Pharm Res 34:2084-2096.

655 28. Leung SY, Parumasivam T, Gao FG, Carrigy NB, Vehring R, Finlay WH, Morales S,
656 Britton WJ, Kutter E, Chan H-K. 2016. Production of inhalation phage powders using
657 spray freeze drying and spray drying techniques for treatment of respiratory infections.
658 *Pharm Res* 33:1486-1496.

659 29. Leung SSY, Parumasivam T, Gao FG, Carter EA, Carrigy NB, Vehring R, Finlay
660 WH, Morales S, Britton WJ, Kutter E, Chan H-K. 2017. Effect of storage conditions on
661 the stability of spray dried, inhalable bacteriophage powders. *Int J Pharm* 521:141-149.

662 30. Leung SSY, Parumasivam T, Nguyen A, Gengenbach T, Carter EA, Carrigy NB,
663 Wang H, Vehring R, Finlay WH, Morales S, Britton WJ, Kutter E, Chan H-K. 2018.
664 Effect of storage temperature on the stability of spray dried bacteriophage powders. *Eur*
665 *J Pharm Biopharm* 127:213-222.

666 31. Leung SSY, Carrigy NB, Vehring R, Finlay WH, Morales S, Carter EA, Britton WJ,
667 Kutter E, Chan H-K. 2019. Jet nebulization of bacteriophage with different tail
668 morphologies – structural effects. *664:322-326*.

669 32. Muttill P, Wang C, Hickey AJ. 2009. Inhaled drug delivery for tuberculosis therapy.
670 *Pharm Res* 26:2401-2416.

671 33. Xiong X, Zhang HM, Wu TT, Xu L, Gan YL, Jiang LS, Zhang L, Guo SL. 2014. Titer
672 dynamic analysis of D29 within MTB-infected macrophages and effect on immune
673 function of macrophages. *Exp Lung Res* 40:86-98.

674 34. Hatfull GF. 2014. Mycobacteriophages: windows into tuberculosis. *PLoS Pathog*
675 10:e1003953.

- 676 35. Froman S, Will DW, Bogen E. 1954. Bacteriophage active against virulent
677 mycobacterium tuberculosis I. isolation and activity. Am J Public Health Nations Health
678 44:1326-1333.
- 679 36. Nadithe V, Rahamatalla M, Finlay WH, Mercer JR, Samuel J. 2003. Evaluation of
680 nose-only aerosol inhalation chamber and comparison of experimental results with
681 mathematical simulation of aerosol deposition in mouse lungs. J Pharm Sci 92:1066-
682 1076.
- 683 37. Leong BKJ, Coombs JK, Sabaitis CP, Rop DA, Aaron CS. 1998. Quantitative
684 morphometric analysis of pulmonary deposition of aerosol particles inhaled via
685 intratracheal nebulization, intratracheal instillation or nose-only inhalation in rats. J Appl
686 Toxicol. 18:149-160.
- 687 38. Wolff, RK. 2015. Toxicology studies for inhaled and nasal delivery. Mol Pharm
688 12:2688-2696.
- 689 39. Phillips JE. 2017. Inhaled efficacious dose translation from rodent to human: a
690 retrospective analysis of clinical standards for respiratory diseases. Pharmacol Ther
691 178:141-147.
- 692 40. Phalen RF. 1976. Inhalation exposure of animals. Environ Health Perspect 16:17-
693 24.
- 694 41. Liu K-Y, Yang W-H, Dong X-K, Cong L-M, Li N, Li Y, Wen Z-B, Yin Z, Lan Z-J, Li W-
695 P, Li J-S. 2016. Inhalation study of mycobacteriophage D29 aerosol for mice by
696 endotracheal route and nose-only exposure. J Aerosol Med Pulm Drug Deliv 29:393-
697 405.

698 42. Semler DD, Goudie AD, Finlay WH, Dennis JJ. 2014. Aerosol phage therapy
699 efficacy in *Burkholderia cepacia* complex respiratory infections. *Antimicrob Agents*
700 *Chemother* 58:4005-4013.

701 43. Kutter E, Sulakvelidze A. 2005. *Bacteriophages: biology and applications*. CRC
702 Press, Boca Raton, USA.

703 44. Hoe S, Semler DD, Goudie AD, Lynch KH, Matinkhoo S, Finlay WH, Dennis JJ,
704 Vehring R. 2013. Respirable bacteriophages for the treatment of bacterial lung
705 infections. *J Aerosol Med Pulm Drug Deliv* 26:317-335.

706 45. Jacobs-Sera D, Marinelli LJ, Bowman C, Broussard GW, Guerrero Bustamante C,
707 Boyle MM, Petrova ZO, Dedrick RM, Pope WH, SEA-PHAGES, Modlin RL, Hendrix
708 RW, Hatfull GF. 2012. On the nature of mycobacteriophage diversity and host
709 preference. *Virology* 434:187-201.

710 46. Kanjee Z, Amico KR, Li F, Mbolekwa K, Moll AP, Friedland GH. 2012. Tuberculosis
711 infection control in a high drug-resistance setting in rural South Africa: information,
712 motivation, and behavioral skills. *J Infect Public Health* 5:67-81.

713 47. Roach DR, Leung CY, Henry M, Morello E, Singh D, di Santo JP, Weitz JS,
714 Debarbieux L. 2017. Synergy between the host immune system and bacteriophage is
715 essential for successful phage therapy against an acute respiratory pathogen. *Cell Host*
716 *Microbe* 22:38-47.

717 48. Bowen LE, Rivers K, Trombley JE, Bohannon JK, Li SX, Boydston JA, Eichelberger
718 MC. 2012. Development of a murine nose-only inhalation model of influenza:

719 comparison of disease caused by instilled and inhaled A/PR/8/34. *Front Cell Infect*
720 *Microbiol* 2:74.

721 49. Wheeler AJ, Ganji AR. 2010. *Introduction to engineering experimentation*, 3rd
722 edition. Pearson Higher Education, Upper Saddle River, NJ, USA.

723 50. Ochs M, Nyengaard JR, Jung A, Knudsen L, Voigt M, Wahlers T, Richter J,
724 Gundersen HJ. 2004. The number of alveoli in the human lung. *Am J Respir Crit Care*
725 *Med* 169:120-124.

726 51. Guirado E, Mbawuiké U, Keiser TL, Arcos J, Azad AK, Wang S-H, Schlesinger LS.
727 2015. Characterization of host and microbial determinants in individuals with latent
728 tuberculosis infection using a human granuloma model. *mBio* 6:e02537-14.

729 52. Żaczek M, Łusiak-Szelachowska M, Jończyk-Matysiak E, Weber-Dąbrowska B,
730 Międzybrodzki R, Owczarek B, Kopciuch A, Fortuna W, Rogóż P, Górski A. 2016.
731 Antibody production in response to staphylococcal MS-1 phage cocktail in patients
732 undergoing phage therapy. *Front Microbiol* 7:1681.

733 53. Van Belleghem JD, Dąbrowska K, Vaneechoutte M, Barr JJ, Bollyky PL. 2019.
734 Interactions between bacteriophage, bacteria, and the mammalian immune system.
735 *Viruses* 11:10.

736 54. Fauvart M, De Groote VN, Michiels J. 2011. Role of persister cells in chronic
737 infections: clinical relevance and perspectives on anti-persister therapies. *J Med*
738 *Microbiol* 60:699-709.

739 55. Fairchild GA. 1972. Measurement of respiratory volume for virus retention studies in
740 mice. *Appl Microbiol* 24:812-818.

741 56. Martin AR, Ang A, Katz IM, Häussermann S, Caillibotte G, Texereau J. 2011. An *in*
742 *vitro* assessment of aerosol delivery through patient breathing circuits used with medical
743 air or a helium-oxygen mixture. *J Aerosol Med Pulm Drug Deliv* 24:225-234.

744 57. Kuehl PJ, Anderson TL, Candelaria G, Gershman B, Harlin K, Hersterman JY,
745 Holmes T, Hoppin J, Lackas C, Norenberg JP, Yu H, McDonald JD. 2012. Regional
746 particle size dependent deposition of inhaled aerosol in rats and mice. *Inhal Toxicol*
747 24:27-35.

748 58. Soutiere SE, Tankersley CG, Mitzner W. 2004. Differences in alveolar size in inbred
749 mouse strains. *Respir Physiol Neurobiol* 140:283-291.

750 59. Larsen SE, Baldwin SL, Orr MT, Reese VA, Pecor T, Granger B, Dubois
751 Cauwelaert N, Podell BK, Coler RN. 2018. Enhanced anti-*Mycobacterium tuberculosis*
752 immunity over time with combined drug and immunotherapy treatment. *Vaccines*
753 (Basel) 6:30.

754 60. Bertholet S, Ireton GC, Ordway DJ, Windish HP, Pine SO, Kahn M, Phan T, Orme
755 IM, Vedvick TS, Baldwin SL, Coler RN, Reed SG. 2010. A defined tuberculosis vaccine
756 candidate boosts BCG and protects against multidrug-resistant *Mycobacterium*
757 *tuberculosis*. *Sci Transl Med* 2:53ra74.

758 61. Saini D, Hopkins GW, Seay SA, Chen CJ, Perley CC, Click EM, Frothingham R.
759 2012. Ultra-low dose of *Mycobacterium tuberculosis* aerosol creates partial infection in
760 mice. *Tuberculosis (Edinb)* 92:160-165.

761 62. Gern B, Plumlee C, Gerner M, Urdahl K. 2017. Investigating immune correlates of
762 protection to tuberculosis using an ultra-low dose infection in a mouse model. Open
763 Forum Infect Dis 4:S47-S48.